

Perflutren lipid microsphere injectable suspension for cardiac ultrasound

Echocardiography is a widely available noninvasive procedure for diagnosing cardiovascular disease. With the development of clinically useful microbubble contrast agents to enhance echocardiographic images and advantages of portability without radiation, microbubble contrast agents have become essential established adjunctive tools to perform state-of-the-art echocardiography. Several manufacturers produce commercially available stabilized microbubbles for intravenous use. Perflutren lipid microsphere (DEFINITY®) is one of the second generation microbubble contrast agents approved for left ventricular opacification and left ventricular endocardial border detection, and is the subject of this review.

KEYWORDS: contrast echocardiography endocardial border definition eleft ventricular opacification eperflutren lipid microsphere estress echocardiography eltrasound microbubble contrast agents

Contrast imaging was introduced to diagnostic ultrasound more than 40 years ago [1]. The first ultrasound contrast agent described in the late 1960s was agitated saline. More than two decades were required to develop a microbubble contrast agent (MCA) that consisted of a high molecular weight gas encapsulated by an insoluble shell. These MCAs can be injected intravenously and circulate throughout the systemic circulation to produce an excellent arterial blood pool effect, termed left ventricular opacification (LVO) and left ventricular endocardial border detection (EBD) [2,3]. Successful evaluations of MCAs were undertaken by a number of researchers and pharmaceutical companies in both animals and human clinical trials. Incremental benefits of improved accuracy and reproducibility for assessment of left ventricular (LV) function have been demonstrated with the use of MCAs in both stress and rest transthoracic echocardiography (TTE) [4]. It was also shown that the use of MCA for LVO may contribute to a more cost-effective pattern of patient care [5].

In addition to LVO, microbubbles can be deliberately disrupted by the ultrasound beam and the rate at which fresh microbubbles replenish the scan plane can be observed in subsequent images, thus enabling the quantification of microvascular flow rate and relative vascular volume. Although the use of MCAs for myocardial perfusion has been extensively researched, it has not yet been routinely implemented in clinical practice and is limited to off-label use and in research studies. In addition to MCA use in echocardiography, noncardiac application of contrast ultrasound imaging has expanded the range of spatial and temporal resolution in radiological ultrasound diagnostics [6].

In 2008, the American Society of Echocardiography (ASE) guidelines provided the rationale of MCA use for the purposes of improving endocardial visualization in all subjects with two or more suboptimal contiguous LV wall segments. In addition, the guidelines highlighted specific clinical scenarios requiring the use of MCA to obtain the best diagnostic information [2]. Subsequently, in 2009, the European Association of Echocardiography [7], similarly documented the clinical value of MCAs. In 2010, the Intersocietal Commission for the Accreditation of Echocardiography Laboratories (ICAEL) affirmed the necessity of MCA availability and skilled use for laboratory accreditation and further emphasized the need for a written policy per individual laboratories for the use of MCAs or for alternative imaging if MCAs were not used [101]. In addition, the use of MCAs has been acknowledged in the 2011 American College of Cardiology/ASE Appropriateness Criteria for TTE [8]. Subsequently, the International Ultrasound Contrast Society [102] was organized to provide cohesive information on MCAs in different ultrasound fields.

To date, the US FDA has approved two perfluoropropane MCAs for the indications of EBD and LVO in patients with suboptimal baseline images. These commercially available MCAs include: FSO 69 (OPTISONTM; GE Healthcare Inc., Princeton, NJ, USA), which was approved in 1998 and DMP 115 (DEFINITY[®]; Lantheus

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Medical Imaging, North Billerica, MA, USA), which was approved in 2001. These and several other MCAs are approved for use in other parts of the world [2].

This article will focus on commercially available perflutren lipid microsphere injectable suspension pharmacologic properties and evidence from the literature on efficacy and safety. Additional highlights from major studies of the off-label use of these agents will be also discussed.

Overview of ultrasound contrast agents

The commercial development of MCAs began in the 1980s with the first agent Echovist[®] (Schering, Berlin, Germany), which enabled right ventricle enhancement but it did not survive passage through the pulmonary circulation [9]. In 1985, Levovist[®] (Schering, Berlin, Germany), a galactose palmitic acid encapsulated air microbubbles was developed and approved in Europe, Japan and Canada. Both Albunex[®] (Molecular Biosystems Inc., San Diego, CA, USA) and Levovist are transpulmonary MCAs but with a reduced longevity *in vivo* (half-life <5 min) resulting in less than optimal LVO [10]. In North America, the production of Albunex enabled LVO after an intravenous injection [11]. Albunex was the first agent approved by the FDA in 1994.

With increasing recognition of the potential usefulness of MCAs, the focus shifted to the production of stabilized shelf-ready microbubbles. An increasing number of manufacturers produced forms of stabilized MCAs with smaller diameter $(\leq 10 \ \mu m)$ able to cross the pulmonary circulation, having a longer effect. To achieve a persistent clinically useful effect, small amounts of high molecular weight gases known as perfluorocarbons (PFCs) were utilized. PFCs (i.e., perfluorocarbon, perfluorobutane, perfluoropropane, and perfluorohexane) are inert compounds with a low surface tension, and can be intravenously injected if emulsified. These 'second generation' MCAs containing PFCs demonstrated clear superiority to earlier agents with respect to the degree and duration of LVO, EBD and Doppler enhancement, and further as off-label use for myocardial perfusion [12]. TABLE 1 illustrates the current market overview

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Table 1. Perfluorochemical-containi	14 IIICI ODUDDIE COITCASCA	uenits, mistory and	ינטוו כווג אנמנטא.

Trade name	Research name	Shell	Gas [molecular formula]	Manufacture (location)	US FDA approval	Approved indication
Optison™	FSO 69	Albumin	Octafluoropropane [C ₃ F ₈]	GE Healthcare Inc. (Princeton, NJ, USA)	1998	LVO and EBD
DEFINITY®	DMP 115	Phospholipids	Octafluoropropane $[C_{3}F_{8}]$	Lantheus Medical Imaging (North Billerica, MA, USA)	2001	LVO and EBD
lmagent®	AF0150	Surfactant	Perfluorohexane $[C_6F_{14}]$	Alliance Pharmaceutical Corporation (San Diego, CA, USA)	2002	LVO and EBD (never commercially available for clinical applications)
SonoVue®	BR1	Surfactant	Sulfur hexafluoride [SF ₆]	Bracco Diagnostic (Milan, Italy)	NA	LVO, EBD and Doppler (approved in Europe, some Latin American and Asian countries)
Sonazoid®	NC100100	Lipid	Decafluorobutane $[C_4F_{10}]$	Amersham Imaging (GE Healthcare, Oslo, Norway) Daiichi Sankyo (Tokyo, Japan)	NA	CEU imaging of hepatic lesions (approved in Japan on January 2007)
EchoGen®	QW3600	Surfactant	Dodecafluoropentane $[C_5F_{12}]$	SONUS Pharmaceuticals (Bothell, WA, USA)	NA	Withdrawn from development in 2001
PESDA	Perfluorocarbon- exposed sonicated dextrose albumin	Sonicated albumin/ dextrose	Decafluorobutane $[C_4F_{10}]$	Thomas Porter/ University of Nebraska (Omaha, NE, USA)	NA	Not commercially developed
Imagify™	AI-700	Synthetic polymer	Decafluorobutane [C₄F₁₀]	Acusphere (Watertown, MA, USA)	NA	IND for MCE

of PFCs containing MCAs. Latest research efforts are ongoing to develop microbubbles for molecular imaging (third generation agents) and for targeted drug/gene delivery (fourth generation agents) as a site-specific, ultrasound directed, drug or gene therapeutic tool [13].

Concomitantly, unique contrast-specific imaging techniques that are now routinely available on ultrasound machine platforms were being developed. Indeed, the ultrasound market has experienced a dynamic transition over the last decade driven by the need for enhanced contrast detection. The primary mechanisms for MCA signal enhancement are microbubble backscattering, oscillation and rupture, all of which are primarily dependent on the acoustic power (mechanical index) of the transmitted ultrasound beam. These improvements have enabled not only excellent visualization of MCAs within cardiac chambers but also within the myocardial microvasculature [2].

The only commercially available perflutren lipid microsphere injectable suspension in the USA is DEFINITY, approved by FDA in July 2001 and was also approved by the European Medicine Agency in September 2006 under the name LUMINITY® (Lantheus Medical Imaging, North Billerica, MA, USA). Up to this date, 3.3 million patients have received DEFINITY, for contrast-enhanced echocardiographic procedures since the first product approval [103].

Introduction to the compound ■ Chemistry

The main two components of DEFINITY, include a core of perflutren gas (octafluoropropane and perfluoropropane) and an outer lipid shell. The chemical name (molecular formula) for perflutren is 1,1,1,2,2,3,3,3-octafluoropropane $[C_3F_8; CF_3-CF_2-CF_3]$. Its molecular weight is 188.02 g/mol. It is a colorless and odorless gas that is chemically inert and thermally stable because of the strength of the carbon–fluorine bond. FIGURE 1 shows the structural formula of the active substance in DEFINITY.

The lipid shell is composed of three phospholipids (0.75 mg/ml) including DPPA (1,2-dipalmitoyl-sn-glycero-3-phosphatidic acid, monosodium salt); DPPC (1,2-dipalmitoyl-sn-glycero-3-phosphatidylcholine); and MPEG5000 DPPE: *N*-(methoxypolyethylene glycol 5000 carbamoyl)-1,2-dipalmitoyl-sn-glycero-3-phosphatidylethanolamine, monoso-dium salt. DPPA and DPPC are major constituents of human cell membranes. DPPA negatively charges the microspheres reducing coalescence.

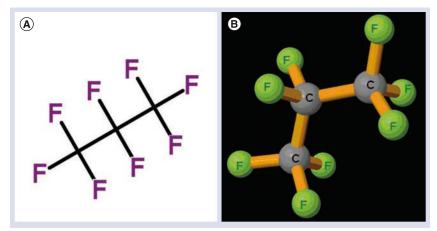


Figure 1. Structural formula of the active substance (perflutren gas) in **DEFINITY®** $[C_3F_8]$. (A) Drawing of the chemical structure. (B) 3D reconstruction of the chemical structure of the octafluoropropane showing three carbon atoms.

Other ingredients included in the formulation matrix are phosphate buffer (for phospholipid stability purposes); sodium chloride (used as a tonicity agent); propylene glycol (improves the hydrophilic properties of the phospholipids during compounding); and glycerol (increases viscosity and stability) [14,103].

Pharmacodynamics

Mechanism of DEFINITY actions

Activated DEFINITY is small enough to pass through the lungs and circulate in the vascular system. The difference in density and compressibility between the MCA and the surroundings creates an efficient reflector of the ultrasound beam, thus enhancing blood echogenicity and EBD [15]. The mechanical index is a major parameter affecting

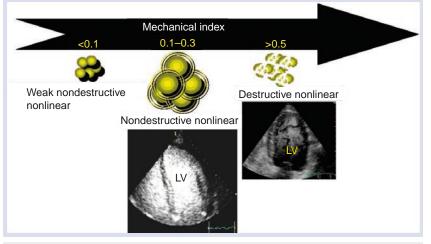


Figure 2. Microbubble behavior in ultrasound field based on mechanical index. At mechanical index (0.1–0.3), the four-chamber view shows homogenous left ventricular enhancement and good endocardial border delineation. At a mechanical index of >0.5, the microbubbles are destroyed and swirling is seen in the left ventricular cavity. LV: Left ventricle.

Table 2. Pharma	acokinetic characte	ristics of DEFINITY [®] .			
C _{max} (µl/ml)	C _{max} achieved t	ime (min) CL (l/h)	t	1⁄2 (min)	Dose excreted in expired air (%)
			Healthy subjects	COPD subjects	
0.79–9.52	1–2	1088–4775	1.3	1.9	15–85% (mean ~50%)
CL: Clearance rate; C _{ma}	x: Maximum concentration;	COPD: Chronic obstructive lung dis	ease; t ½: Half-life	2.	

microbubble oscillation [2]. These oscillations can result in weak nonlinear backscatter at a very low mechanical index (<0.1); nonlinear signals (ultraharmonics) at low-medium mechanical index (0.1-0.5); and microbubble destruction at high mechanical index (>0.5) where the shell is broken and the gas rapidly diffuses into the surroundings [16]. FIGURE 2 illustrates microbubble behavior in an ultrasonic field as a function of mechanical index. In general, the acoustic properties of activated DEFINITY are characterized by improved stability and favorable resonance behavior at or below a mechanical index of 0.8 [103]. While conventional 2D ultrasound can detect high concentrations of microbubbles, in practice optimal assessment requires contrast-specific imaging modes. These specific ultrasound modes are based on the cancellation and separation of the linear signals arising from tissue and utilization of the nonlinear response from MCA [17]. Detection of the nonlinear response from DEFINITY was observed with variable underlying imaging approaches including conventional harmonic imaging, subtraction techniques performed using single pulse (coherent imaging mode), or multiple pulses (pulse or phase inversion mode) and combined for multiframe subtraction techniques. The characteristics of activated DEFINITY response to ultrasound waves and its effectiveness in enhancing ultrasound imaging for LVO and myocardial perfusion were established in animal models and several human clinical trials [2]. A correlation between increased mechanical index and decreased persistence of DEFINITY microbubbles in circulation was demonstrated both in *in vitro* and *in vivo* models [15]. DEFINITY was shown to exhibit a peak mean backscatter power at concentrations between 1 and 10×10^6 microbubbles/ml with a linear reduction of mean backscatter power in concentrations lower than this [18]. The persistence of clinically useful LVO was demonstrated for approximately 3.4 min for activated DEFINITY bolus dose (3-10 µl/kg) and 7 min for continuous diluted infusion in 50 ml normal saline (10 µl/kg, at a rate of 4 ml/min). Such effects permit the interrogation of multiple views during an echocardiographic study. Although higher DEFINITY doses

have been shown to produce a longer LVO effect, definite dose-response relationship could not be a established [19,20].

Hemodynamic & tissue effects of DEFINITY in preclinical & clinical studies

It was observed that the activated DEFINITY microbubbles had identical velocity to red blood cells within the arterioles, capillaries and venules, and no obstruction of the vessels occurred [21,22]. The effects of activated DEFINITY on cardiovascular hemodynamics was evaluated in preclinical studies in pigs at dose levels ranging from 0.5 to 10 µl/kg showing no changes in heart rate, systemic pressure or arterial oxygen saturations. However, a mild reversible increase in pulmonary arterial pressure was observed [23,24]. Such a dose (10 µl/kg) is currently the highest recommended dose for clinical use [103]. In a multicenter randomized, placebo-controlled, double-blind trial study by Kitzman and colleagues in patients with suboptimal baseline echocardiographic images, two doses of activated DEFINITY (5 vs 10 µl/kg) were given. The study showed no clinically significant change in hemodynamic, electrocardiography or hematological values between the two dosage groups [3]. The differences in hemodynamic responses between humans and pigs are attributed to unique species-specific thromboxane release from porcine pulmonary intravascular macrophages, which induces pulmonary hypertension. Indeed, Szebeni proposed that the pig represents a highly sensitive testing model for assessing hypersensitivity reactions [25], although the extrapolation to humans who do not have pulmonary intravascular macrophages is not clinically relevant. In a prospective controlled human clinical study by Wei et al., no changes in peak or mean pulmonary arterial pressures were observed using invasive monitoring after a full dose of DEFINITY in patients with normal or elevated predose pulmonary arterial pressures [26].

Studies examining the effect of activated DEFINITY on cerebral vasculature utilizing histopathological sections of the brain indicated no adverse effect seen at doses that are five-times that of the human dose within 5 min

Table 3. Se	Table 3. Selected pivotal DEFINITY $^{\circ}$ Phase III clinical	I DEFINITY	[®] Phase III clir	nical trials.								
Study	Design	Number of centers	Number of patients	Number of controls	Age I (mean (± SD)	Males (%)	DEFINITY dose	Outcome evaluated	Follow-up safety visit (h)	Outcome	ome	Ref.
										% of subjects with optimal LV enhancement, median (range)	% of segments with change in evaluability, median (range)	
DEFINITY® Study-004	Randomized, double-blind, multicenter, placebo- controlled	o	69	18	62.5 ± (12.3	69 (79.3) 5 and 10 µ/И	5 and 10 µl/kg	LV enhancement EBD improvement	24, 48 and 72	60.6%† (60.6–63.6%)	9.4 [‡] (2.3–24.0%)	[105]
Kitzman <i>et al.</i> (2000)	Randomized, double-blind, multicenter, placebo- controlled	17	169	24	56 ± 6.3	140 (66)	5 and 10 µl/kg	LV enhancement EBD improvement	24, 48 and 72	61.2%† (42.9–77.6%)	13.4* (13.1–13.8%)	[3]
Weissman et al. (2000)	Open-label, multicenter, cross-over trial	m	64	0	60.9 ± ² 15.7	45 (70.3)	Two boluses 10 µl/kg Single infusion in 50 ml saline	LV enhancement Compare bolus vs infusion	24 and 72	Bolus 98% [§] (76–98%)	Infusion 96% [§] (77–93%)	[20]
[†] Statistically sig [‡] Statistically sig [§] Statistically sig EBD: Endocardi	¹ Statistically significant difference from placebo (p < 0.01). ¹ Statistically significant change in evaluability (p < 0.05). ⁸ Statistically significant difference from baseline images (p < 0.01). EBD: Endocardial border delineation; LV: Left ventricle; SD: Standard deviation.	<i>irom placebo (p < valuability (p < 0 irom baseline imč n; LV: Left ventri</i>	< 0.01). 1.05). ages (p < 0.01). cle; SD: Standard d	le viation.								

Study of ageMeans (%) ageIndication testIndex testComparator testI segment modelE diagnostic yieldRef.Kurt63263.6396 (62.7)Patients with baseline suboptimal imagesEchocardiogram with DEINITYI segments model with DTI segments model testI segments model testI segments model tertancialy difficult studies decreased from tertancialy difficult studies decreased from 1.6 to 99.9% (p < 0.0001)301Nayar596434 (57.6)Patients with baseline suboptimal imagesEchocardiogram with DEINITY Number of abnormal segments visualized increased from 2.5 ± 48 to 3.8 ± 6.5393Nayar596434 (57.6)Patients with baseline with DEINITY with DEINITY with outEchocardiogram test and equate studies from 1.6 to segments (p < 0.0001)303Nayar596434 (57.6)Bernet with baseline with DEINITY segments (p < 0.0001)303Nayar596434 (57.6)Bernet with baseline segments (p < 0.0001)303Nayar596434 (57.6)Bernet with Baseline segments (p < 0.0001)303Nayar596434 (57.6)C.5.3354Nayar646464646466Sood images and LVWith DEINITYWith Out C.C.33C.C.3367Sood images and LVBernet With determined with C.C.33C.C.33C.C.33Sood6434C.C.33C.C.11Sood64 </th <th>. Pivotal</th> <th></th> <th></th> <th></th> <th></th> <th></th> <th></th> <th></th> <th></th>	. Pivotal								
63.6 396 (62.7) Patients with baseline with DEFINITY® without suboptimal images Echocardiogram with DEFINITY® without in the suboptimal images Interpretable studies decreased from	umber f atients	Mean age	Males (%)	Indication	Index test	Comparator test	LV segment model	CE diagnostic yield	Ref.
64 34 (57.6) Patients with baseline Echocardiogram Echocardiogram 16-segment model Proportion of variation in LV EF in good images and LV with DEFINITY without EF determined with NCE: 21 dysfunction DEFINITY NCE, NCC, CE and CC NCC: 33 CE: 25 CC: 11 CC: 11	332	63.6	396 (62.7)	Patients with baseline suboptimal images	Echocardiogram with DEFINITY®	Echocardiogram without DEFINITY	17 segments model	Uninterpretable studies decreased from 11.7 to 0.3% Technically difficult studies decreased from 86.7 to 9.8% Increase in adequate studies from 1.6 to 89.9% (p < 0.0001) Number of abnormal segments visualized increased from 2.5 ± 4.8 to 3.8 ± 6.5 segments (p < 0.0001)	[30]
	29	64	34 (57.6)	Patients with baseline good images and LV dysfunction	Echocardiogram with DEFINITY				[31]

of administration. Although another study in rats looking at a different PFC-based MCAs revealed disruption of the blood-brain barrier that lasted 24 h [27]. A study investigating the influence of perflutren on microvessels in the rat mesentery and myocardium reported no evidence of microvessel bleeding and/or endothelial cell injury unless high mechanical index ultrasound exposure occurred [21]. While mechanistic reports studying the potential for hypersensitivity response of the immune system to DEFINITY, suggested possible complement factor (C3a) activation as an immediate response, declining gradually over 30 min, the actual mechanism has not been clearly established [104].

Pharmacokinetics

DEFINITY is presented as a vial containing a translucent liquid phospholipid mixture with octafluoropropane gas in the head space. After activation (emulsification) using a mechanical shaking device (Vialmix[®], Lantheus Medical Imaging, North Billerica, MA, USA) for 45 s, it becomes an opaque suspension (1 ml of the milky white dispersion contains a maximum of 1.2×10^{10} perflutren lipid microspheres with a diameter ranging from 1.1 to 3.3 µm, and approximately 1.1-mg/ml octafluoropropane) [104].

The pharmacokinetics of an intravenous dose of activated DEFINITY was evaluated in healthy humans and those with chronic obstructive pulmonary disease. Using validated gas chromatographic methods, perflutren gas was found to mainly be cleared by the lungs in the expired air in an unchanged state. The rapid elimination of perflutren gas in the expired air was also consistent with the rapid disappearance of ultrasound contrast enhancement after activated DEFINITY administration. Furthermore, there were no statistically significant differences observed in the concentration-time curves of blood perflutren in normal versus chronic obstructive pulmonary disease subjects [104,105]. The lipid shell contains both DPPC and DPPA, which are endogenous lipids that are metabolized to free fatty acids. MPEG5000 DPPE is not an endogenous phospholipid and is cleared from the circulation via urine as MPEG5000 [19]. TABLE 2 shows the pharmacokinetic characteristics of DEFINITY.

Clinical efficacy

We review below the pivotal Phase I, II and III studies that were conducted in support of the use of DEFINITY for contrast-enhanced echocardiography.

Phase I studies

Two Phase I clinical trials were performed to determine the safety and tolerance of a single ascending dose or multiple doses of DEFINITY in 30 and 18 healthy adult male subjects, respectively [28]. These Phase I trials further assessed the contrast enhancement of the cardiac chambers visually and by quantitative videodensitometric measurements. The efficacy results of these Phase I studies indicated that both median visual scores for contrast enhancement and mean changes from baseline in quantitative videodensitometric measurements were higher in the DEFINITY-treated group compared with the placebo group. Both studies reported on the hemodynamic safety with no treatment-related changes in vital signs, ECG or arterial oxygen saturation (15 min-24 h after DEFINITY administration) and that the doses were well tolerated in humans with no significant side effects [28].

Phase II studies

Pantely and colleagues evaluated 19 patients referred for diagnostic echocardiography in a Phase II study [29]. DEFINITY was administered as a single intravenous bolus injection at doses of 5, 10 or 15 μ l/kg. Optimal enhancement was observed for approximately 1.5–2 min in the 10- μ l/kg dose group, while excessive attenuation occurred in the 15- μ l/kg dose group. Based on these findings, the dose of 5–10 μ l/kg was recommended for use in the Phase III efficacy cardiology trials.

Phase III studies

Three pivotal Phase III multicenter clinical trials on DEFINITY were evaluated by the FDA [3,20,105]. These were performed in patients with known or suspected cardiac disease and suboptimal (≥ 2 nonevaluable segments) echocardiographic images with doses ranging from 5 to 10 µl/kg. Outcomes evaluated were the percentage of subjects who demonstrated optimal LVO and the percentage of segments with change in evaluability from nonevaluable at baseline to evaluable post-DEFINITY. In all trials, subjects with optimal LVO intensity were higher in the contrast than in noncontrast (placebo) groups. No serious adverse events were reported, however, the most frequent new-onset adverse events (≥1%) were fatigue, dyspnea, headache, chest pain, flushing, nausea and dizziness. Furthermore, no dose relationship could be detected for the overall frequency of treatment-related, new-onset adverse events in subjects receiving bolus doses of DEFINITY.

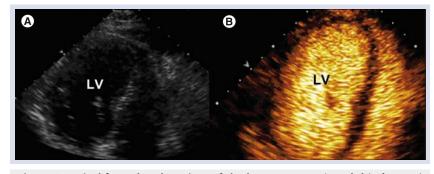


Figure 3. Apical four-chamber view of the heart. Images show (A) before and (B) after contrast enhancement showing a uniform contrast left ventricular opacification permitting complete endocardial border detection and visualization of all endocardial segments. LV: Left ventricle.

TABLE 3 illustrates the results of pivotal DEFINITY Phase III trials that were submitted to the FDA for approval.

DEFINITY was further evaluated in two abdominal ultrasound Phase III multicenter clinical trials enrolling 209 patients (130 with suspected liver pathology and 79 with suspected kidney pathology). The authors concluded that the addition of the DEFINITY contrast agent to standard grayscale abdominal ultrasound provided both additional diagnostic information and substantive changes in patient management, with 23% of patients judged to not require additional diagnostic examinations [14].

Clinical applications of contrast echocardiography

DEFINITY is approved in the USA for use in suboptimal echocardiograms [103] and use of MCAs is required for echocardiography laboratory accreditation [101].

Enhancement of endocardial border during rest TTE

Beyond enhanced endocardial visualization, the use of MCA for quantification of LV volumes and ejection fraction (EF) has been shown to have excellent correlation with comparative imaging modalities, demonstrating improved intra- and inter-observer agreement and physician interpretation confidence [2]. In addition to the two pivotal Phase III trials identified above [3,20], two additional studies in which DEFINITY was used to enhance resting TTE confirmed these findings [30,31]. TABLE 4 SUMMARIZES DEFINITY studies demonstrating the benefit of contrast utilization for LVO during resting TTE. These studies [3,30] further assessed the direct impact of contrast-enhanced echocardiography on health outcomes in patients requiring assessment of ventricular function. Kitzman and colleagues

Table 5. P	Table 5. Pivotal DEFINITY® studies during stress transthoracic echocardiography.	tudies durin	ig stress tra	insthoracic ec	nocargiograph	×.					
Study	Patients number Mean age (C/NC) (years)	Mean age (years)	Males (%)	Indication	Index test	Reference (cutoff)	LV segment model	Sensitivity (%)	Specificity (%)	Accuracy (%)	Ref.
Moir et al. (2004)	85, 70 underwent CA C: 70 NC: 70	57.0	61 (87)	Patients with suspected CAD	Dipyridamole- ESE with DEFINITY vs NC dipyridamole- ESE	CA (≥50%)	16	NC: 74 CE: 86	NC: 81 CE: 81	ЧN	[36]
Plana <i>et al.</i> (2008) OPTIMIZE trial	101 C: 101 NC: 101	59.6	80 (79)	Patients with intermediate- high risk of CAD	C DSE with DEFINITY vs NC DSE	CA (≥70%) 17	17	CE: 80 NC: 75	CE: 55 NC: 51	CE: 66 NC: 53	[35]
Dolan <i>et al.</i> (2009)	Total of 5934 underwent CA C: 4011 NC: 1923	70.0	C: 61.4 NC: 58.2	Patient with suspected CAD	Contrast DSE or ESE with DEFINITY or OPTISON TM vs NC DSE or ESE	CA (≥50%) 17	17	CE: 81 NC: 73	AA	CE: 82 NC: 77	[34]
C: Contrast; CA: NC: Noncontrast.	C: Contrast; CA: Coronary angiography; CAD: Coronary artery disease; CE: NC: Noncontrast.	CAD: Coronary ar	tery disease; CE:		Contrast estimated; DSE: Dobutamine stress echocardiography; ESE: Exercise stress echocardiography; LV: Left ventricle; NA: Not available;	ess echocardiogr	aphy; ESE: Exercise	stress echocardiogi	raphy; LV: Left ventric	cle; NA: Not availa	le;

concluded that the use of DEFINITY provided information that eliminated the need for additional testing in 60% of patients and aided EF determinations in 81% of all patients when compared with those who received placebo [3]. These rates of salvaged echocardiographic studies were in a similar range to other MCAs (51% for perflenapent emulsion [32] and 74% for albumin perfluoropropane microbubbles [12]). It is notable that these findings were obtained even in the era of fundamental imaging, prior to optimization of ultrasound imaging technology as is routinely used today for enhanced MCA detection. In the landmark paper by Kurt and colleagues, the use of DEFINITY for LVO significantly impacted diagnostic accuracy, resource utilization and directly benefited patient management [30]. Such benefit was reflected in change of therapy, procedure or both in 35.6% of suboptimal quality studies. FIGURE 3 illustrates on apical four-chamber view pre- and post-contrast enhancement showing uniform LVO and EBD with improved visualization of all endocardial segments.

Enhancement of endocardial border during stress TTE

The use of MCAs with stress echocardiography (SE) improves the diagnostic accuracy of stress echo in the diagnosis of coronary artery disease (CAD) [33]. Several nonrandomized studies compared noncontrast with contrast SE utilizing DEFINITY [34-37] or albumin perfluoropropane microbubbles [38-44] primarily to identify wall motion abnormalities in clinically indicated SE studies. TABLE 5 summarizes pivotal studies utilizing specifically DEFINITY for LVO in SE.

Other studies utilizing different PFC-based MCAs have shown similar results. Using an albumin perfluoropropane MCA, Thanigaraj and colleagues, reported that 53% of patients with poor resting images who underwent SE were referred to subsequent nuclear stress testing versus 3% of those who received MCA [41]. Furthermore, two studies [45,46] utilizing an airbased MCA (Levovist) demonstrated the value of contrast-enhanced SE over noncontrast SE for the prediction of total cardiac events [47,48]. FIGURE 4 depicts an apical two-chamber view preand post-contrast enhancement, demonstrating the effect of uniform LVO with MCA to allow complete visualization of endocardial segments and detection of regional wall motion abnormalities in the apical and mid-anterior wall, not otherwise seen on noncontrast images, and correlating with significant coronary artery stenosis confirmed at coronary angiography.

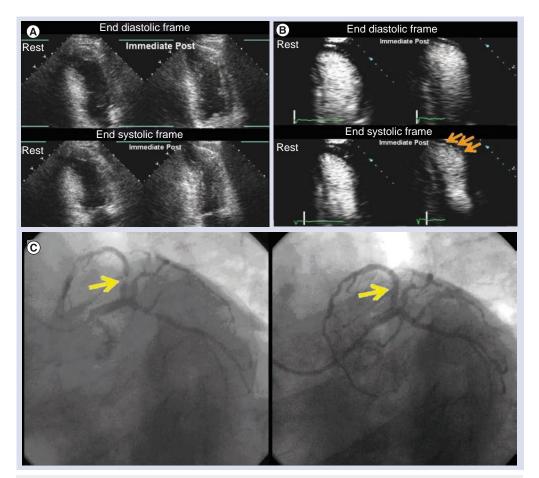


Figure 4. Treadmill echocardiography showing (upper panels) apical two-chamber view at rest and immediate post stress in both end diastolic and end systolic frames. Images acquired (A) without contrast and (B) after contrast enhancement (grouped arrows). Regional wall motion abnormalities in the apical-mid anterior wall are more clearly visualized on the contrast images. (C) Coronary angiography showing: 90% stenosis (arrow) of left anterior descending coronary artery, post-stenting: there is no further evidence of left anterior descending stenosis.

The very clear endocardial border definition that occurs with MCA has allowed enhanced observation not only of systolic abnormalities of wall thickening, but also diastolic abnormalities. These regional diastolic contour alterations of the endocardium provide incremental information to detect the presence of angiographically significant CAD compared with LV systolic wall thickening abnormalities alone [49]. FIGURE 5 demonstrates Regional diastolic contour alterations that were observed in the apical four-chamber view (apical region) during immediate post-stress imaging; a significant coronary stenosis was confirmed at angiography.

Assessment of abnormal cardiac structural anatomy & hemodynamic flow

MCAs are of value in the detailed structural assessment of the left and right ventricles, the atria and the great vessels [2]. In particular, the diagnoses of apical LV pathology (e.g., apical variant of hypertrophic cardiomyopathy and thrombus), postmyocardial infarction complications (e.g., LV rupture or pseudoaneurysm, or ventricular septal defect) and intracardiac masses [50] are significantly enhanced. Suboptimal Doppler signals and their spectral envelopes can be clearly demarcated to permit determination of peak velocities and time velocity integrals, in order to improve assessment of right ventricular systolic pressures, valvular stenosis, intracardiac shunts and diastolic function [2].

Off-label use of DEFINITY for myocardial perfusion

MCAs enhance the backscattered ultrasound signals and can be seen not only in the LV cavity, but also in the myocardium. Thus, myocardial perfusion can be detected, and quantified using MCA. A growing number of published articles have documented the use of DEFINITY and other MCAs for use as myocardial perfusion

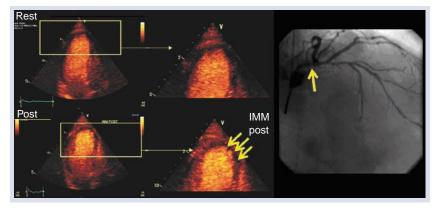


Figure 5. Apical four-chamber view illustrating the novel sign of regional diastolic contour abnormalities during a treadmill echocardiography. Left panel (lower): the immediate post-exercise stage shows an apical wall motion abnormality, and regional diastolic contour abnormalities sign (arrows) observed in the mid-to-apical septum (zoomed apical region) in comparison to resting images (upper) showing no wall motion abnormality and a smooth apex. Right panel: coronary angiography showing 70% stenosis of distal left main (arrow) and a proximal 80% left anterior descending artery stenosis. IMM post: Immediate post-exercise; Post: Post-exercise; Rest: At rest.

agents to detect perfusion abnormalities both at rest and in conjunction with exercise and pharmacological SE [51-59]. The fundamental concept for evaluation of perfusion using real-time contrast echocardiography is dependent on the instantaneous depletion (destruction) of microbubbles and observation of their gradual refill (replenishment) into the myocardial microvasculature. We and others have performed metaanalyses to evaluate the diagnostic accuracy of contrast echocardiography for detection of perfusion abnormalities quantitatively [60] and qualitatively [61]. Dijkmans and colleagues reported [61] that perfusion abnormalities detected by myocardial perfusion echocardiography showed equivalent noninferior results to those of SPECT dobutamine SE for the detection of CAD. An example of normal myocardial perfusion as evaluated by myocardial contrast echocardiography is illustrated in FIGURE 6. We have also reported on the pooled sensitivity and specificity for the quantitative perfusion parameters of myocardial blood flow velocity reserve (β) and coronary flow

reserve (Aβ reserve) as: 81% (95% CI: 76–85) and 77% (95% CI: 73–80), and 80% (95% CI: 75–84) and 81% (95% CI: 77–84), respectively [60]. An example of a myocardial perfusion defect observed using myocardial perfusion echocardiography is shown in FIGURE 7. Selected SE studies utilizing DEFINITY for evaluation of myocardial perfusion with coronary angiography and/or SPECT as a reference standard test for CAD diagnosis is shown in TABLE 6 with reported range for sensitivities and specificities of 67–91% and 51–96%, respectively.

A prognostic role of myocardial perfusion during SE has been demonstrated in multiple studies. Tsutsui and colleagues studied 788 patients with real-time myocardial perfusion during dobutamine SE with a median follow-up of 20 months [62]. The authors reported that abnormal myocardial perfusion had significant incremental value over clinical factors, resting EF and wall motion in the prediction of cardiac events. In addition, Dawson and colleagues, in a study enrolling patients with known or suspected CAD and comparing dipyridamole perfusion echocardiography with simultaneous SPECT, noted that during a mean follow-up period of 14 months, abnormal perfusion echocardiography was found to be an independent predictor of adverse cardiac outcome (odds ratio: 23, 95% CI: 6-201; p < 0.001) and further provided an incremental prognostic value over clinical variables, LV systolic function, inducible wall-thickening abnormalities and SPECT results [63].

Cost–effectiveness of DEFINITY

Several studies have evaluated the cost–effectiveness of MCAs by comparing outcomes within patients undergoing echocardiography with and without MCA [5,40,64]. Moir and colleagues utilized DEFINITY for LVO during pharmacologic and/or exercise SE in 135 patients undergoing coronary angiography. The authors noted that LVO was of benefit to 14% of patients, unrelated to resting image quality. They also reported on



Figure 6. Dobutamine stress echocardiography. Apical four-chamber view at peak stress demonstrating normal myocardial perfusion with homogenous DEFINITY[®]. **(A)** Contrast enhancement of the myocardium before flash, **(B)** microbubbles destruction (flash) and **(C)** complete replenishment by 3 s after flash.

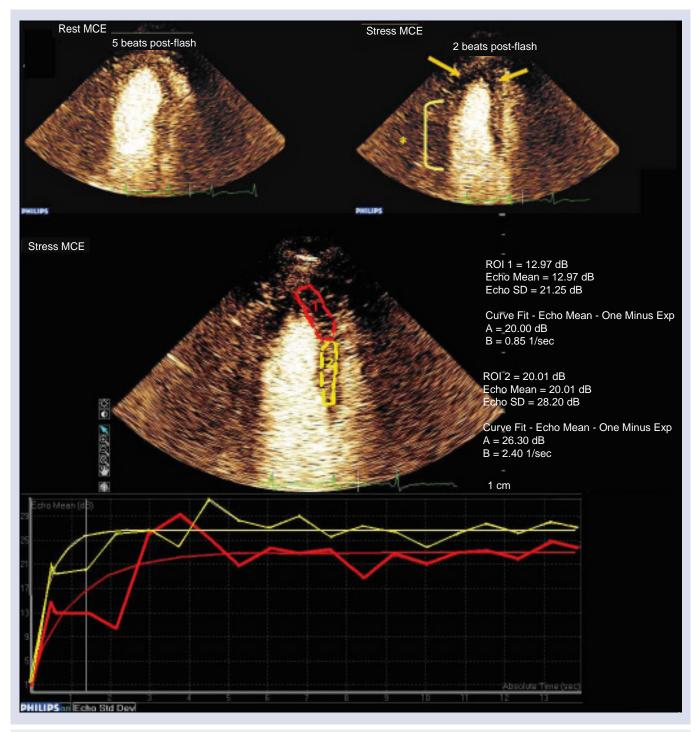


Figure 7. Representative example of qualitative and quantitative myocardial contrast echocardiography analysis. Upper panel: apical four-chamber view five beats postflash at rest (left) showing homogenous myocardial enhancement; while apical perfusion defect is seen two beats postflash during peak stress (right, arrows). There is an artifactual 'drop out' segment in the lateral wall (*). Lower panel: time–intensity curves are shown fitted to mono exponential function, $Y = A (1-e^{-\beta i})$, where Y is video intensity at pulsing interval t; β (sec¹) represents rate of rise in signal intensity (microbubble velocity) and A (dB) is peak plateau of videointensity (myocardial blood volume) obtained from apical four-chamber view at peak stress with two ROI quantifying the defect and the normal adjacent segment. ROI 1 (red) in apical region where the perfusion defect shows A = 20.0 dB and β of 0.85 s⁻¹ while ROI 2 (yellow) shows A parameter = 26.30 dB and $\beta = 2.40$ s⁻¹. ROI: Region of interest; SD: Standard deviation.

improvement of sensitivity from 80 to 91%, p = 0.03, while nonsignificant improvement in specificity was observed (72–77%; p = 0.25) [64].

Despite that, the authors concluded that the use of DEFINITY was not cost effective in all patients; however, their methods were limited

<u>o</u> .	patients	;	agent	for significant CAD	(%)	Keported diagnostic yield	кет.
Porter <i>et al.</i> 1. (2001) (4	117 (40 had CA)	Dobutamine	DEFINITY: 19 OPTISON™: 98	CA (>50%)	30 (25.6)	Accuracy: MCE: 83%; WM: 72%	[22]
Elhendy <i>et al.</i> 13 (2004) (1	1318 (179 had CA)	Dobutamine	DEFINITY: 30 OPTISON: 140	CA (≥50%)	127 (75)	Sensitivity: MCE: 91%; WM: 70% Specificity: MCE: 51%; WM: 74%	[78]
Moir et al. 8 (2004)	85	ESE-dipyridamole	DEFINITY	CA (≥50%)	42 (51)	Sensitivity: WM: 74%; MCE and WM: 91% Specificity: WM: 81%; MCE and WM: 70%	[36]
Tsutsui e <i>t al.</i> 24 (2005) (1 N 24	2498 (1486 received MCA) and of those 249 had CA	Dobutamine	DEFINITY: 35% OPTISON: 65%	CA (>50%)	180 (72.3)	Sensitivity: MCE: 96%; WM: 64% Specificity: MCE: 51%; WM: 72% Accuracy: MCE: 84%; WM: 66%	[37]
Elhendy <i>et al.</i> 1. (2005)	128 ⁺	Dobutamine	DEFINITY:41 OPTISON: 87	CA (≥50%)	101 (79)	MCE: sensitivity: 89%; specificity: 52%; accuracy: 81%	[62]
Moir <i>et al.</i> 9 (2005)	06	ESE-dipyridamole	DEFINITY	CA (≥50%)	48 (53)	Sensitivity: MCE qualitative: 93%; MCE quantitative: 88% Specificity: MCE qualitative: 65%; MCE quantitative: 52%	[80]
Tsutsui <i>et al.</i> 3((2005) (1	36 (16 had CA)	Dipyridamole	DEFINITY	SPECT CA (≥50%)	SPECT: 20 (56) CA: 13 (36)	MCE vs SPECT ⁺ : sensitivity: 70%; specificity: 81%; accuracy: 75% MCE vs CA ⁺ : sensitivity: 67%; Specificity: 92%; accuracy: 85%	[81]
Elhendy <i>et al.</i> 6. (2006)	64	Dobutamine	DEFINITY: 26 OPTISON: 38	CA (≥70%)	49 (77)	MCE ^s · sensitivity: 74%; specificity: 79%; accuracy: 77%	[82]
Toledo <i>et al.</i> 3. (2006)	34	Dipyridamole	DEFINITY	CA (≥70%)	25 (73.5)	MCE quantitative for LAD: sensitivity: 83%; specificity: 67%; accuracy: 75% MCE quantitative for non-LAD: sensitivity: 71%; specificity: 67%; accuracy: 70%	[83]
Xie <i>et al.</i> (2007) 40	0	Adenosine	DEFINITY	SPECT CA (>50%)	29 (72.5)	MCE vs SPECT: sensitivity: 76%; specificity: 94%; accuracy: 83% MCE vs CA: sensitivity: 78%; specificity: 86%; accuracy: 90%	[84]
Abdelmoneim 9. <i>et al.</i> (2010) fe	91 (88 were feasible for analysis)	Adenosine	DEFINITY	SPECT	42 (46)	Abdelmoneim 91 (88 were Adenosine DEFINITY SPECT 42 (46) MCE vs SPECT: sensitivity: 88%; [8] et al. (2010) feasible for analysis) WM vs SPECT: sensitivity: 62%; WM vs SPECT: sensitivity: 62%;	[85]

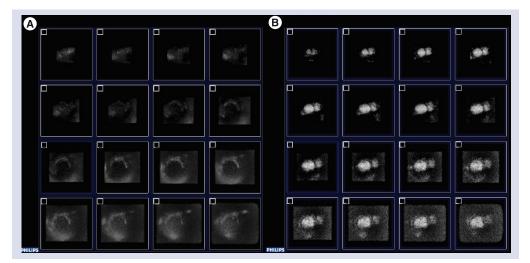
only to assessment of improvement in diagnostic accuracy in order to neutralize the cost of the intervention (contrast agent) and did not take into account the clinical impact and cost-savings in avoidance of additional downstream testing. In another study of 315 patients (277 received contrast vs 38 patients with no contrast) undergoing SE and SPECT studies, a net US\$238 saving in the group receiving MCA was reported [41]. Other cost-effectiveness analyses by Shaw and colleagues [5], revealed 2.7-fold improvement in the diagnostic accuracy for patients with a nondiagnostic echocardiogram receiving contrast, with a cost saving of \$319 per patient. Furthermore, Kurt and colleagues illustrated the impact of utilizing contrast echocardiography on the clinical management of 632 consecutive patients with technically difficult echocardiographic studies. The authors reported 32.8% of patients in whom additional diagnostic procedures were avoided, and alteration of drug management in 10% and concluded with a savings using contrast agent of \$122 per patient on a cost-benefit analysis [30].

New technology with contrast echocardiography

The diagnostic accuracy of echocardiography has been enhanced by the combined advances in 3D contrast echocardiography [65]. Recent improvements in 3D contrast technology include the incorporation of power modulation imaging, which provides incremental benefit for visualization of microbubbles in the myocardial microcirculation and significant advantages in image acquisition time [66]. We and others have reported on the preliminary observations of feasibility and potential benefit of 3D over 2D echocardiography in the assessment of myocardial perfusion utilizing DEFINITY [66-68]. 3D transducer technology improvements including increased operating frequency and bandwidth, transducer miniaturization, and flash technology have been developed, and continue to be refined. FIGURE 8 demonstrates 3D echocardiographic short axis views in 16 segments I-slice cropping format, base to apex, pre- and post-contrast enhancement. Complete LVO with improved visualization of all endocardial segments can be seen.

Postmarketing surveillance

Postmarketing surveillance is mandated by the FDA for routine postapproval monitoring of drug safety. As part of this process, a sequence of events occurred that have affected labeling of the MCA class. A 'box warning' was placed in October 2007 after rare fatalities (n = 4) and uncommon serious cardiopulmonary adverse events (n = 197) thought to be temporally related to the administration of MCA were reported [104]. This action followed that in Europe, as the European Medicine Agency halted use of a sulfurhexafluoride-based MCA for similar concerns [106]. In May 2008, after review of the accumulated safety data, including additional safety reports on larger cohorts of patients, validations of the usefulness of MCA in patient management and cost-effectiveness, the FDA revised the labeling changes to reflect the established clinical safety record of MCAs [104]. More recently, in May 2011, the FDA has





Ref.	C vs NC: within 72 h. Death 1 vs 2 [86] (p = 0.54). MI: 3 vs 7 (p = 0.92) within 30 days. Death 37 vs 57 (p = 0.85) MI 17 vs 16 (p = 0.19) cong term: adjusted HR between C and NC. Death: 0.99 (95% CI: 0.88–1.11), MI: 0.99 (95% CI: 0.80–1.22)	NC: MI 0 vs 3 [87] vs 1. No VF. No	vents. Serious [88] s in four	No fatalities. Serious nonfatal reactions [89] in eight. Anaphylactoid reactions in four	C vs NC: deaths 0 vs 2 (p = 0.1). [76] Serious adverse events 0.19 vs 0.17% (p = 0.7). Sustained VT 8 vs 8 (p = 0.32). Cardiac arrest 2 vs 2 (p = 0.96)	No sustained VT, VF, cardiac arrest or [90] death in either group. C vs NC: MI: 1 vs 0 anaphylactoid reaction 1 vs 0 (p = 0.51). Significant arrhythmias: 2.1 vs 1.9% (p = 0.8)	vithin 30 min in [34] h. One death and n contrast group. Death: 37 vs 62 ss 73 (p = NS). Long
Event rate (%)	C vs NC: within 72 h. Death 1 vs 2 (p = 0.54). MI: 3 vs 7 (p = 0.92) within 30 days. Death 37 vs 57 (p = 0.85) MI 17 vs 16 (p = 0.19) Long term: adjusted HR between C and NC. Death: 0.99 (95% CI: 0.88–1.11), MI: 0.99 (95% CI: 0.80–1.22)	No fatalities. C vs NC: MI 0 vs 3 sustained VT in 1 vs 1. No VF. No anaphylaxis	No fatalities. 20 events. Serious nonfatal reactions in four	No fatalities. Serious nonfatal rea in eight. Anaphylactoid reactions in four	C vs NC: deaths 0 vs 2 ($p = 0.1$). Serious adverse events 0.19 vs 0 ($p = 0.7$). Sustained VT 8 vs 8 ($p = 0.32$). Cardiac arrest 2 vs 2 ($p = 0.96$)	No sustained VT, VF, cardiac arrest death in either group. C vs NC: MI: 1 vs 0 anaphylactoid reaction 1 vs (p = 0.51). Significant arrhythmias: 2.1 vs 1.9% (p = 0.8)	No deaths or MI within 30 min in either group <24 h. One death and five nonfatal MI in contrast group. C vs NC: 30 days. Death: 37 vs 62 (p = NS). MI: 68 vs 73 (p = NS). Long
Outcome of interest	Short-term (72 h and 30 days) and long-term (4.5 years) death or MI	Immediate adverse events	Adverse events within 30 min	Adverse events within 30 min	Death in 24 h, adverse events within 30 min	Immediate adverse events	Death and Ml within 30 min, 24 h, long-term outcome (25 months)
Number of patients receiving DEFINITY®	9300 (86%)	54%	12,974	66,164	2811 (59%)	1971 (67.6%)	12,802 (68% of SE)
Number of patients (C vs NC)	C: 10,792 NC: 15,982	C: 1150 NC: 2554	C: 16,025 NC: 0	C: 78,383 NC: 780,243	C: 4786 NC: 5012	C: 2914 NC: 2155	C: 42,408 NC: 23,812
Echocardiography	SE	SE	Rest TTE, SE	Rest TTE, SE, general, ultrasound	SE	SE	Rest TTE, SE
Population included	Outpatients	Inpatients with stable chest pain and in those with suspected ACS	Outpatients, inpatients and ICU patients	Outpatients and inpatients	95% outpatients	Outpatients	Outpatients and inpatients
Number of patients	26,774	3704	112,776	858,626	9798	5069	66,220
Study period	2003- 2007	2004– 2008	1998– 2007	2001– 2007	1998– 2007	1999– 2007	1999– 2007
Study	Abdelmoneim et al. (2009)	Anantharam et al. (2009)	Herzog (2008)	Wei <i>et al.</i> (2008)	Gabriel et al. (2008)	Shaikh <i>et al.</i> (2008)	Dolan <i>et al.</i> (2009)

Table 7. Reports on the safety of ultrasound contrast agents used during echocardiography (cont.).		e salety of							
Study	Study period	Number of patients	Population included	Echocardiography Number of patients (C vs NC)	Number of patients (C vs NC)	Number of patients receiving DEFINITY®	Outcome of interest	Event rate (%)	Ref.
Main <i>et al.</i> (2008)	2002– 2007	4,300,966	Premier perspective database, hospitalized patients	Rest TTE	C: 4,242,712 NC: 58,254	58,254	Death within 24 h	C vs NC: deaths 616 vs 45,789 (p = 0.613), adjusted odds ratio of 0.76 (95% CI: 0.70–0.82)	[91]
Kusnetzky et al. (2008)	2005– 2007	18,671	Hospitalized patients	Rest TTE	C: 6196 NC: 12,475	6196	Death within 24 h	C vs NC: deaths 26 vs 46 (p = 0.60)	[92]
Aggeli <i>et al.</i> (2008)	2002	5250	Outpatients	SE	C: 5250 NC: 0	¢	Adverse events within 24 h	No fatalities. No MI. Sustained VT or VF requiring resuscitation in two sustained VT not requiring resuscitation in 10. Nonsustained VT in 18. Anaphylactoid reactions not requiring hospitalization in 23	[93]
[†] All study group ACS: Acute coro TTE: Transthorac	received SonoV nary syndrome; ic echocardiogr	All study group received SonoVue TM contrast agent. ACS: Acute coronary syndrome; C. Contrast, Cl. Con ITE: Transthoracic echocardiography; VF: Ventricular	ient. Confidence interval; cular fibrillation; VT: \	'All study group received SonoVue ^{tw} contrast agent. ACS: Acute coronary syndrome; C: Contrast; CI: Confidence interval; HR: Hazard ratio; ICU: Intensiv TTE: Transthoracic echocardiography; VF: Ventricular fibrillation; VT: Ventricular tachycardia.	/e care unit; MI: M	yocardial infarction,	: NC: Noncontrast; NS: Noi	¹ All study group received SonoVue ^{tw} contrast agent. ACS: Acute coronary syndrome; C: Contrast; Cl: Confidence interval; HR: Hazard ratio; ICU: Intensive care unit; MI: Myocardial infarction; NC: Noncontrast; NS: Nonsignificant; SE: Stress echocardiography; TTE: Transthoracic echocardiography; VF: Ventricular fibrillation; VT: Ventricular tachycardia.	

again revised DEFINITY label (see safety data) [104]. At present, the only contraindications to DEFINITY are those originally placed in the label, including patients with known hypersensitivity or those with known or suspected right-to-left or bidirectional shunts.

Safety

Several reviews have indicated that all the ultrasound MCAs have microscale bioeffects in vivo when given at sufficient concentrations and exposed to higher ultrasound energy for longer times [69]. Two main bioeffect concerns included the increased frequency of premature ventricular contractions and the possibility of vascular injury and cardiac injury [70,71]. These were associated mostly with imaging at a high mechanical index [72,73]. However, these bioeffects were not reported with low mechanical index imaging [37]. Given the physical and chemical structure similarities of the MCA, the safety risks for one agent of class microbubbles may represent risks for all members of the drug class. The body of evidence drawn from large databases followed the FDA box warning, aiming to evaluate the safety of PFC-based MCA. TABLE 7 reports on the safety published studies on MCA focusing on DEFINITY.

In a recent meta-analysis of published studies (up to October 2009) on the adverse cardiovascular events (myocardial infarction and all-cause mortality) with MCAs [74], the authors noted that the cumulative evidence was not suggestive for any MCA-related increase in the incidence of mortality or myocardial infarction with a pooled odds ratio of 0.57 (95% CI: 0.32-1.01; p = 0.05); and 0.85 (95% CI: 0.35-2.05; p = 0.72), respectively.

In response to the FDA call for postmarketing registries to evaluate clinical outcomes and potential MCA serious adverse events, two recent Phase IV studies were conducted and presented at the ASE 21st Annual Scientific Sessions. Additionally the data were presented in the FDA joint meeting of the Cardiovascular and Renal Drugs Advisory Committee and the Drug Safety and Risk Management Advisory Committee discussing perflutren lipid microsphere in May 2011 [107]. The CARES multicenter safety registry was one of the Phase IV studies implemented in the setting of routine clinical practice per MCA guideline indications. The CARES study evaluated all adverse events within 30 min and 24 h of DEFINITY administration including life-threatening cardiopulmonary events in 1053 dosed patients (mean age:

 61.3 ± 12.9 years) at 15 USA sites. This study reported no deaths or life-threatening events at 24 h post-DEFINITY [107].

Reported findings on pulmonary hemodynamics in preclinical studies [23,24] on pigs raised additional concerns regarding the possibility of increased risk for serious cardiopulmonary reactions in patients with significant pulmonary hypertension and receiving MCA. In response to the FDA call for postmarketing registries to evaluate safety in patients with pulmonary hypertension, Wei and colleagues presented a prospective multicenter open-label nonrandomized, placebo-controlled Phase IV safety study in 32 patients (mean age: 57.2 ± 12.9) [26]. The authors evaluated pulmonary and systemic hemodynamics invasively in patients with (pulmonary artery systolic pressure, [PASP] >35 mmHg) and without pulmonary hypertension (PASP ≤35 mmHg) and receiving DEFINITY. No deaths or serious adverse events were reported. In addition, no change in PASP hemodynamics was associated with DEFINITY [107]. However, this study excluded patients with baseline PASP of >75 mmHg.

We [75] and others [76] have also demonstrated the safety of MCAs in pulmonary hypertension patients. Gabriel and colleagues reported no evidence of serious adverse events in 57 patients with moderate-to-severe pulmonary hypertension (right ventricular systolic pressure >50 mmHg) who underwent SE [76]. Our group has also reported no significant difference in short- or long-term events (4.6 years) between the contrast and noncontrast cohorts, with an adjusted hazard ratio (95% CI) for death and myocardial infarction of 1.10 (0.80–1.50; p = 0.56) and 0.34 (0.11–1.03; p = 0.06), respectively [75].

Following the DEFINITY safety data presented for FDA review in September 2010 and in May 2011, the boxed warning contained within the DEFINITY label was re-revised in respect to patients with pulmonary hypertension or unstable cardiopulmonary conditions, in whom the 30 min post-DEFINITY monitoring was no longer required. In addition, the committee concurred with the safety and efficacy data presented for DEFINITY during exercise and pharmacologic stress testing and hence the statement regarding lack of such evidence was removed. Furthermore, a new label change included a statement about serious reactions uncommonly occurring but if they do, it would usually be within 30 min of administration, which negates the need for additional monitoring beyond the timeframe of performing the echocardiographic study [104].

Regulatory affairs

DEFINITY was approved in Canada for use with echocardiography and radiology in December 2000 and in the USA in 2001 for use with echocardiography only. It is also available for echocardiographic and or radiologic use in Latin America, Europe, Australia and some Asian countries [104].

Conclusion

Based on data available from original publications, reviews and guidelines, the use of MCA with echocardiography in patients with suboptimal images is considered part of standard clinical echocardiographic practice and is supported by ultrasound professional societies (ASE, International Contrast Ultrasound Society, ICAEL). Test feasibility and performance, confidence of interpretation, and cost-effectiveness is significantly greater with contrast enhancement when indicated. After rigorous evaluation, DEFINITY MCA has demonstrated a good safety profile with documented benefit, and low risk, which is comparable to other noninvasive imaging modalities, with the distinct advantages of portability, lack of nephrotoxicity or radiation risk.

Future perspective

MCAs provide an established tool in contemporary echocardiography practice. Clinical applications for the use of MCAs for LVO and EBD are well established and regulated. The off-label applications of MCA for evaluation of myocardial perfusion, as well as perfusion of noncardiac vascular beds as assessed in radiologic imaging, are being evaluated in numerous clinical trials, while also being utilized daily

Executive summary

Perflutren lipid microsphere injectable suspension (DEFINITY[®]; DMP 115) is a class of intravenously injectable perfluoropropane-based ultrasound contrast agents.

Mechanism of action

- Activated DEFINITY is an efficient reflector of ultrasound beam, thus enhancing blood echogenicity and improving the delineation of endocardial borders.
- The acoustic properties of activated DEFINITY are characterized by improved stability and favorable resonance behavior at or below a mechanical index of 0.8.
- DEFINITY permits the use of echocardiography to visualize and localize myocardial perfusion defect (off-label use).

Pharmacokinetic properties

- After administration of activated DEFINITY, the perflutren gas is cleared by the lungs unchanged and the lipid shell metabolized to free fatty acids.
- The half-life of perflutren gas is 1.3 min in healthy subjects and 1.9 min in subjects with chronic obstructive pulmonary disease.

Clinical efficacy

- DEFINITY microbubble contrast agent is used to:
- Improve the diagnostic accuracy, confidence of interpretation, and reduce intra- and inter-observer variability in the evaluation of left ventricular systolic function, quantification of LV volumes and ejection fraction in patients with technically challenging suboptimal echocardiograms
- Improve the assessment of segmental wall thickening and increase diagnostic accuracy during stress echocardiography
- Confirm or exclude the presence of apical left ventricle pathology, assist in detection and classification of suspected intracardiac masses and evaluate mechanical complications after myocardial infarction
- Enhance inadequate Doppler spectral profile

Safety & tolerability

- The incidence of all serious side effects with ultrasound contrast agents is 1:10,000–1:15,000.
- The following are contraindications to DEFINITY ultrasound contrast agents:
- Right-to-left, bidirectional, or transient right-to-left cardiac shunts
- Hypersensitivity to perflutren

Drug interactions

No known drug interactions.

Dosage & administration

- Bolus: the recommended bolus dose is 10 µl/kg of the activated DEFINITY by intravenous bolus injection within 30–60 s, followed by a 10-ml saline flush. If necessary, a second 10-µl/kg dose followed by a second 10-ml saline flush may be administered 30 min after the first injection to prolong contrast enhancement.
- Infusion: the recommended infusion dose is via an IV infusion of 1.3 ml added to 50 ml of preservative-free saline. The rate of infusion should be initiated at 4.0 ml/min, but titrated as necessary to achieve optimal image enhancement, not to exceed 10 ml/min.
- Diluted IV bolus injection: 1.3 ml of activated DEFINITY diluted with 8.7 ml of preservative-free saline in a 10-ml syringe. Initial injection of up to 3 ml administered slowly subsequent injections of 1–2 ml as needed. The maximum permitted dose of activated DEFINITY via this method is one single vial.

in many ultrasound laboratories, avoiding unnecessary radiation exposure, and potential nephrotoxicity. With innovative imaging techniques and the development of newer MCAs, ultrasound contrast imaging has become much more than a technique to rescue technically limited examinations. Designer microbubbles for research applications in tissue-targeted gene or drug therapy, endothelial integrity assessment and ultrasound-enhanced thrombolysis offer very exciting future frontiers.

Financial & competing interests disclosure

S Mulvagh has received research grants from Lantheus Medical Imaging and Astellas Pharma Global Inc. She has been a member of the Advisory Board for GE Healthcare. The authors have no other relevant affiliations or financial involvement with any organization or entity with a financial interest in or financial conflict with the subject matter or materials discussed in the manuscript apart from those disclosed.

No writing assistance was utilized in the production of this manuscript.

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