Razer percutaneous coronary intervention (Rotational and Laser atherectomy) for an undilatable coronary lesion with a under deployed stent

An under expanded stent in a heavily calcified lesion is a technical challenge and a therapeutic dilemma. Under expanded stents are associated with instent restenosis, acute and sub-acute thrombosis and residual angina. Excimer laser (ELCA) has been successfully used in such cases and there are isolated reports of the use rotational atherectomy (RA). There are only few published reports where both these modalities were used together. We report a case in which ELCA with RA (Razer), was used successfully for percutaneous coronary intervention (PCI) of an undilatable coronary lesion with an under deployed stent.

Keywords: Coronary Artery • Ischaemia • PCI • IVUS

Case Presentation

A 65 year old, patient underwent PCI of calcified proximal and mid right coronary artery (RCA) lesions (Figure 1A) [1,2]. Debunking was performed by RA using a 1.5 mm burr (Figure 1B), the lesions were predicated and Resolute Integrity 3.0 mm x 38 mm and 4.0 mm x 15 mm (Medtronic Inc., Minneapolis, USA) stents deployed in an overlapping fashion. At this stage, we noticed that the overlapped segment had not expanded adequately (Figures 1C and 1D) [3]. The unexpanded segment of the stent was post dilated, multiple times with 3.5 mm NC balloon to high pressures (34 atmps) without success. The procedure was stopped at this stage [3,4].

The patient was readmitted electively after one week for PCI with ELCA of the under deployed stented segment. An optical coherence tomography (OCT) demonstrated that the maximal and minimal luminal diameter in the stented segment was 3.57 mm and 1.52 mm, respectively (Figures 1E and 1F). We used 0.9 mm, ECLA catheter with saline flush (X-80, Vitresse, Spectranetics/Advanced Interventional Systems) to modify the under deployed stented segment. After 5, 8 and 12 passes of laser atherectomy catheter (Figure 2A), the lesion was dilated with a 3.0 mm NC balloon, followed by 2.5 mm and 3.5 mm OPN NC balloon to 30 atmps, respectively. All of above attempts did not have any significant impact on the stenosed segment (Figure 2B).

At this stage, we decided to perform RA. Initially we used a 2.0 mm burr. However, the 2.0 mm burr would not cross the distal end of the calcified segment (Figure 2C). Eventually, a 1.5 mm burr successfully crossed the stenosis segment. After multiple passes, the 1.5 mm burr was up sized to 2.0 mm burr. A total of 9 minutes of RA was performed. Following RA the stenosed segment was adequately dilated using a 3.0 mm and 3.5 mm NC balloon (Figure 2D). After predilatation the stenosed segment was stented with a Resolute Integrity 4.0 x 30 mm stent and post dilated with a 4.0 mm NC balloon (Figure 2E). No stent constraint was demonstrated following post dilation angiographically or by intravascular ultrasound (IVUS) (Figure 2F).
Discussion

Debulking to facilitate dilation of calcified lesions prior to stent implantation can be achieved usually by using RA, ELCA, intravascular lithotripsy (IVL) or cutting balloon. Deployment of a stent prior to recognising that the lesion is non-dilatable leads to a nonexpandable, under-deployed stent. Despite the use of high pressure post dilatation these segments can be highly resistant to balloon dilatation.

ELCA consists of a thin, flexible fiber-optic catheter connected to an external laser-generating source, with the tip of the catheter system emitting pulses of laser energy [3]. The absorption of the laser energy by blood and saline leads to fast vapour bubble expansion and implosion intra-luminally, leading to the fragmentation of superficial fibrocalcific deposits, explosive dilation and vessel expansion [5]. The use of saline infusion at the time of laser pulse delivery has been shown to reduce vessel wall injury due to acoustic damage [6]. ELCA increased lumen by both atheroabloration and forced vessel expansion facilitating dilatation of under-deployed stent [7]. However, in this case we could not achieve stent dilatation with ELCA with saline infusion. There are case reports of the use of contrast and high energy ELCA to facilitate expansion of under-deployed stent [5]. The use of contrast leads to larger sized bubbles and may lead to significant vessel injury. Moreover, the stent was deployed one week back and endothelialisation would not have been completed.

There are isolated published reports of the use of RA to abrade the stent and underlying calcification with subsequent drug eluting stent implantation (stentablation) [3,5]. RA leads to differential cutting of the inelastic tissue (calcium, stents) with deflection away from normal elastic tissue. The lumen improvement after RA is due to tissue ablation. Particulate debris of calcium and metal from RA of a deployed stent is generally under 5 to 15 micrometer and is cleared by the reticuloendothelial system. In this case we used ELCA and RA leading to atheroabloration, fibrocalcific fragmentation, vessel expansion following by tissue and stent ablation [3,7]. After ELCA and RA we successfully deployed a drug eluting stent. The procedure was performed without features of ischaemia, dissection, no re-flow or haemodynamic compromised achieving excellent final angiographic and IVUS results.

Conclusion

ELCA with RA (Razer therapy) can be used safely and effectively to facilitate PCI in a nonexpandable, under-deployed stent in a calcified segment.

Disclosure

Dr. Vivek N Kodoth, Dr. Mark Spence and Dr. Paul W. Johnston have no conflict of interest in relation to this manuscript.

References

Case Report
